

### **FLEXIBILIDADE E TENDÃO DE AQUILES: UMA BREVE REVISÃO**

Anelize Cini<sup>1</sup> Cláudia Silveira Lima<sup>2</sup>

**Resumo:** A realização de treino de flexibilidade como rotina em um programa de exercícios é importante para melhorar amplitude de movimento (ADM). Os tendões têm um impacto profundo na função geral do sistema musculoesquelético, influenciam na limitação da ADM, e sua estrutura e propriedades mecânicas podem se beneficiar de protocolos de alongamento. O uso sistemático dos membros inferiores na locomoção fez com que o tendão de Aquiles se tornasse o maior e mais forte tendão do corpo humano. Portanto, entender qual a melhor prescrição e frequência de exercício de flexibilidade para que ocasione alterações nas propriedades tendíneas é essencial para uma rotina de exercícios adequada e eficaz. Sendo assim, o objetivo dessa revisão de literatura foi organizar e discutir publicações sobre as implicações do alongamento do tríceps sural na ADM, bem como sua influência nas propriedades tendíneas. Estudos agudos mostram que tempos contínuos entre cinco e 10 minutos de alongamento estático causam diminuição da rigidez tendínea, o que não é visto em tempos intervalados inferiores a cinco minutos. Os estudos crônicos, por sua vez, também não apresentam resultados significativos na rigidez com protocolos de alongamento intervalados e estudos com protocolos contínuos não foram encontrados. Dessa forma, não é possível saber se um tempo contínuo de alongamento (superior a um minuto) ou um tempo superior a cinco minutos, intervalado, podem influenciar na rigidez tendínea.

**Palavras-chave:** tendão do Calcâneo; amplitude de movimento articular; fenômenos biomecânicos.

Afiliação

<sup>1</sup> Kinesiology and Kinesiotherapy Research Group, Exercise Research Laboratory, School of Physical Education, Physical Therapy and Dance, Universidade Federal do Rio Grande do Sul, Porto Alegre, RS, Brazil. E-mail: [anelizecini@yahoo.com.br](mailto:anelizecini@yahoo.com.br); Phone: +55 54 99967-4342. <http://lattes.cnpq.br/4705932192013284>; <sup>2</sup> Kinesiology and Kinesiotherapy Research Group, Exercise Research Laboratory, School of Physical Education, Physical Therapy and Dance, Universidade Federal do Rio Grande do Sul, Porto Alegre, RS, Brazil. E-mail: [Claudia.lima@ufrgs.br](mailto:Claudia.lima@ufrgs.br). <http://lattes.cnpq.br/4620443354496222>

## **FLEXIBILITY AND ACHILLES TENDON: A BRIEF REVIEW**

**Abstract:** Performing flexibility training in an exercise program is important to improve range of motion (ROM). Tendons have a profound impact on the general function of the musculoskeletal system, influence the limitation of ROM, and its structure and mechanical properties can benefit from stretching protocols. The systematic use of lower limbs in locomotion caused the Achilles tendon to become the largest and strongest tendon in the human body. Therefore, understanding the best prescription and frequency of flexibility exercise leads to changes in tendon properties is essential for an appropriate and effective exercise routine. Thus, the aim of this review was to organize and discuss publications about the implications of triceps surae stretching in ROM, as well as its influence on tendon properties. Acute studies show that continuous stretching times between five and 10 minutes cause decreased tendon stiffness, which is not seen in fractionated stretching times less than five minutes. Chronic studies, in turn, also don't present significant results in stiffness with fractionated times and studies with continuous times were not found. Thus, it is not possible to know if a continuous stretching time (longer than one minute) or a total time longer than five minutes but fractionated, can influence the tendon stiffness.

**Key words:** Achilles tendon; range of motion, articular; biomechanical phenomena

## Introduction

According to the American College of Sports Medicine (2011) (ACSM)<sup>1</sup> it is important to perform flexibility exercises to improve joint range of motion (ROM), postural stability and balance in all age groups, especially in elderly individuals who lose ROM over time.

Optimal musculoskeletal function requires adequate maintenance of movement in all joints, and it is very clear in the literature that resistance training induces structural and mechanical changes in the muscle-tendon unit (MTU)<sup>2</sup>. On the other hand, the flexibility training proves to be effective in increasing ROM in several populations, but it is not yet clear what mechanical changes occur. Two theories are more widely accepted in the literature to explain these gains: theory based on sensor mechanisms (sensory) and changes in non-contractile structures (mechanical)<sup>3</sup>. Sensory theory has been proposed that the increased ROM is due to a modification of sensation, when it is only observable that subject's perception of the ROM final feeling occurred later after stretch application<sup>4</sup>. The mechanical theories include viscoelastic deformation, because the viscous behavior of MTU when they undergo stretch of sufficient magnitude and duration<sup>4</sup>.

However, flexibility is directly influenced by the soft tissue that surrounds the joint (e.g., muscles, joint capsule, ligaments and tendons)<sup>5</sup>. It is known that when passive movement occurs in a joint, the tendon is responsible for part of the deformation observed in the muscle complex antagonist to the evaluated movement<sup>6</sup>.

Tendons have a profound impact on the general function of the musculoskeletal system in its role as a force transmitter from muscle to bone. The systematic use of lower limbs in human locomotion caused the Achilles tendon to become the largest and strongest tendon in the human body<sup>7</sup>.

The tendons, constituted by type I collagen fibers, influence the limitation of ROM and their structure and mechanical properties may benefit from stretching protocols<sup>8</sup>, since they may change in response to the frequency, duration and magnitude of activities. Thus, the use of stretching exercises is indicated to restore ROM and decrease tendon tension<sup>5</sup>, besides contributing to injury prevention by allowing the good functioning of the entire kinetic chain of motion<sup>9</sup>. However, so far, few studies have directly evaluated deformations related to tendon properties during passive stretching<sup>10-11</sup>.

Therefore, understanding the best prescription and frequency of flexibility exercise to

cause changes in tendon properties are essential for a proper and effective exercise routine<sup>12</sup>. Thus, the aim of this literature review was to organize and discuss publications about the implications of triceps surae stretching in ROM, as well as its influence on Achilles tendon properties.

### **Achilles Tendon**

The calcaneal tendon (Achilles tendon) is constituted of the sheaths of connective tissue of the soleus, medial and lateral gastrocnemius muscles, thus forming the triceps surae muscle group, responsible for plantar flexion of the ankle. It is the greatest and most resistant tendon in the human body, yet it is one of the most common sites of overload injury due to its susceptibility to high loads and stress during locomotion<sup>13-14</sup>.

The triceps surae muscle group is most important for performing daily life and sports activities due to its influence on lower limb strength and power output during locomotion<sup>9,14</sup>. Thus, the tendon receives significant mechanical loads for the purpose of storing and returning elastic energy, thus allowing explosive movements like running and jumping<sup>15</sup>. It is exposed to a considerable stress load in its role of power transmission, it is subsequently vulnerable to the development of damage induced by the load<sup>16</sup>.

Limited dorsal flexion due to shortened triceps surae, combined with low strength, may limit an individual's ability to respond to anterior postural disturbances, and thus require more force to control the center of mass. This can prevent normal walking and cause falls in the elderly<sup>17</sup>. In addition, shortening of these muscles it is associated with several lower limb disorders, such as Achilles tendonitis and plantar fasciitis<sup>18</sup>. These factors demonstrate the importance of establishing proper stretching protocols for maintaining and/or increase angle ROM.

### **Mechanical Properties Of The Tendon**

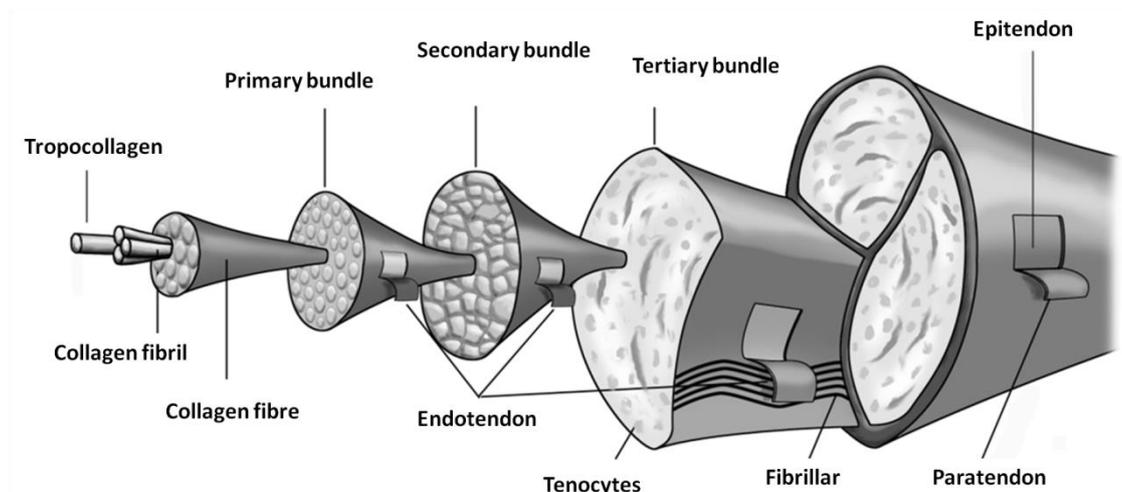
Skeletal muscle are composed of contractile components, the muscle fibers, and elastic components, the aponeurosis, the muscle sheaths (endomysium, perimysium and epimysium) that are constituted after the end of the muscular belly to form the tendon<sup>19</sup>; this set of contractile and elastic components forms the MTU<sup>20</sup>. The tendons, in turn, are white and flexible bands, found forming the origin and insertion of muscles with the function of transmitting muscle strength to the bone<sup>21-22</sup>.

The tendons are also responsible for the storage and release elastic energy during joint movements, which characterizes them as a "biological spring"<sup>11,19,23</sup>. They are constituted by

a complex extracellular matrix, composed of type I collagen and elastin, responsible for traction force, as well as blood and lymphatic vessels and nerves<sup>22</sup>. The collagen fibers, which form the basic unit of the tendon, come from the multiple fibrous sheaths that surround the muscle (endomysium, perimysium, epimysium and fascia) and make it a dense connective tissue structure.

These collagen fibers are grouped into fascicles, which are wrapped by the endotendon. The fascicles are then surrounded by epitendon, which is supplied by blood and lymphatic vessels and nerves; and around it is yet another sheath called paratendon<sup>24</sup>(Figure 1).

The Achilles tendon presents this structural feature, its blood supply is carried by a branch of the posterior tibial artery that provides blood to the peritendinous tissues. The middle portion of the tendon is poorly vascularized. It also receives sensory innervations, especially branches of the sural nerve. Most of the innervations are seen in the paratendon, with little penetration into the epitendon toward the endotendon<sup>25</sup>.



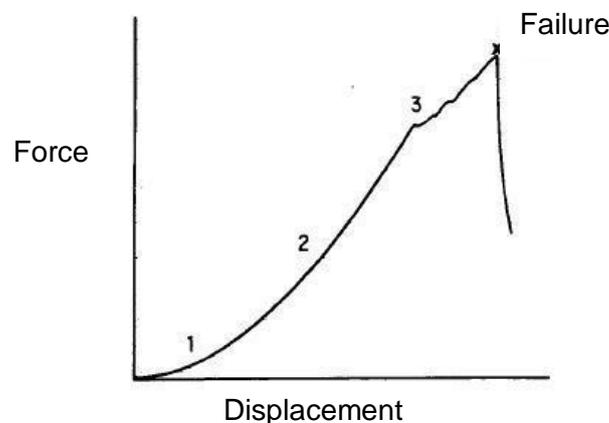
**Figure 1** - Internal architecture of tendon.

When the tendons are studied, the presence of a complex mechanical behavior is observed, namely, the improved range of stretching, resulting from time and history dependent viscoelastic responses.

These responses come from collagen, which as a viscous material, provides flow resistance (e.g., its liquid content provides resistance to movement within the extracellular matrix when stress is applied to this liquid content), defined as viscosity, and affects the load-

deformation curve of these tissues by applying force.

At the beginning of the load-deformation curve (Figure 2-1), the toe region is observed, that is, the collagen fibers, which at rest are wavy begin to distend when force is applied, all crimped fibers straighten. Thus, it is known that when stress is applied, such as when the tendon is stretched, collagen fibers become aligned, causing considerable deformation without using excessive force. By maintaining the overload, after fiber rectification, the linear region or elastic phase begins, where the presented deformation increases linearly with the applied force (Figure 2-2). During this phase the tissue is able to return to its original shape upon removal of the load. In practice, the linear region can be observed when the tissue is taken to the end of its ROM and a smooth stretch is applied. The rhythm of elastic return is determined by the properties of the material, in particular the amount of viscous resistance. It is still possible to observe a yield region, or phase of plastic deformation, which occurs when the elastic limit of the material is exceeded (Figure 2-3). In the yield region the return after load elimination is limited, following a different path than the initial path traveled. Tissue may become permanently deformed due to tissue failure<sup>26</sup>.



**Figure 2** - Tendon load-deformation Curve. (1) toe region; (2) linear region; (3) yield region.

The return path of the load-discharge of the load-deformation curve is called hysteresis, which represents the amount of energy lost in heat during the recoil<sup>27</sup>. By minimizing hysteresis it is possible to increase movement efficiency.

Another aspect that is related to movement efficiency is tendon stiffness. The more compliant the tendon, the greater the ability to stretch and absorb energy. On the other hand, the stiffer a tendon, the more force it takes to increase its length, but the less muscle strength it takes to move a joint.

In turn, because they are constituted by connective tissue, the tendons have the ability to adapt to stimuli, as a result of their plasticity, thus being able to assume a new length after the removal of the initial stimulus. As such, they can benefit from stretching exercise as it leads to increased MTU extensibility and, thereby, increases ROM<sup>8</sup>.

### **Stretching and Tendon**

The absence of regular stretching training and the practice of sports that perform repetitive movements favor a reduction of ROM. The restriction of joint ROM) affects flexibility. This characteristic is considered an intrinsic property of body tissue that depends on the viscoelasticity of muscles, ligaments and other connective tissues, such as tendons<sup>28</sup>.

In sports, problems involving tendons represent a large part of musculoskeletal injuries, such as tendinopathies, being a frequent cause of removal the sports field<sup>22</sup>. Tendinopathies occur when the tissue, on receiving the tension imposed by the movements, cannot deform in order to absorb energy, leading to the onset of micro lesions that over time result in inflammation and rupture.

Factors that are commonly associated with injuries to the musculoskeletal system are excessive stiffness, greater hysteresis, and decreased flexibility in the myotendinous complex<sup>29</sup>. Since stretching can improve these parameters<sup>30</sup>, it is an exercise used to increase ROM, seeking change in viscoelastic tendon behavior<sup>15</sup>.

Static stretching is the most commonly used method to restore or increase flexibility, and is also a therapeutic method for tendinopathy rehabilitation. It is characterized by a slow stretching in the MTU to the point of individual tolerance, maintaining tissue at the at the position of maximum length for a given time<sup>31</sup>. The main advantages of this method over other types of stretching are the low energy application, low risk of exceeding tissue extensibility and unlikelihood of causing pain<sup>5,32</sup>. Stretching only increases ROM when traction is maintained long enough time for the connective tissue to deform, the duration of stretching being directly proportional to the viscoelastic deformation capacity<sup>8</sup>.

Although stretching is a common practice and several studies show increased ROM after its application<sup>33-35</sup>, the evaluation of its efficacy is often restricted to joint movement<sup>36-37</sup>, which limits knowledge regarding the mechanism that leads to this increase<sup>9</sup> often causing the attribution of flexibility gains only to increase the individual's tolerance to stretching<sup>23</sup>.

Knowing that flexibility is influenced by the soft tissues surrounding the joint, e.g. muscles, joint capsule, ligaments and tendons<sup>5</sup>, it is necessary to investigate other outcomes

after stretching in order to obtain more objective information on the behavior of MTU<sup>14,38</sup>.

Stiffness is among the outcomes that allow the assessment of muscle tendon structure behavior. The stiffness of a tissue is determined by the amount of change in the length of this structure when force is applied. The MTU stiffness, as well as muscle and Achilles tendon stiffness are calculated from mathematical formulas that include values of passive torque and myotendinous junction (MTJ) displacement. These outcomes were obtained using an isokinetic dynamometer<sup>37,39-42</sup> and ultrasound<sup>8,37,40-41</sup>, respectively. These outcomes, for the ankle, are measured during passive movements of this joint between the neutral (0°) position and a maximum dorsal flexion.

Stretching with acute protocols of one to two minutes duration has not shown significant results in MTU stiffness<sup>43</sup>, while longer times, between two and a half and three minutes, show a decrease in this stiffness<sup>44</sup>. In addition, studies show that, although MTU stiffness decreases immediately after static stretching at times between two and 8 minutes, this reduction is temporary, since after 20 minutes of rest the stiffness returns to basal level<sup>38</sup>.

Hypotheses are presented to explain the mechanism responsible for this decrease in MTU stiffness induced by stretching, namely: it increases tendon compliance, that is, it decreases tendon stiffness<sup>45</sup>; increases length of muscle fascicle<sup>44</sup>; and/or alteration of intramuscular connective tissue<sup>37</sup>.

Due to the possible interference of tendon stiffness in MTU stiffness, recent studies have begun to evaluate the effect of stretching on tendon stiffness acutely (one intervention) and chronically (after stretching protocols ranging from days to weeks).

### **Acute Effects**

Acute studies (Table 1) show that times between five and 10 minutes of continuous static stretching cause decreased tendon stiffness measured by ultrasound<sup>45-46</sup>. In studies with a shorter and fractionated stretching time protocol, however, tendon stiffness does not change after stretching<sup>9,39,47</sup>. These results suggest that it is necessary to perform stretching for a longer time to have an effect on tendon stiffness.

**Table 1** – Characterization of studies on the acute effect of passive static stretching on the mechanical properties of the Achilles tendon.

| STUDY  | PARTICIPANTS         | STRETCHING PROTOCOL  | RESULTS  |
|--|----------------------|----------------------|--|
| Kay and Blazeovich, 2009a <sup>9</sup>                   | 15, male and female  | 3 x 1 min (rest 60s) | - No difference in tendon stiffness.   |
| Kay, Husbands-Beasley and Blazeovich, 2015 <sup>47</sup> | 17, male and female  | 4 x15 s              | - Increased ROM.<br>- No difference in tendon stiffness and PT.<br>- Decreased muscle stiffness and MTU. |
| Konrad, Stafilidis and Tilp, 2017 <sup>39</sup>          | 122, male and female | 4 x 30 s (rest 20 s) | - Increased ROM.<br>- No difference in tendon stiffness.<br>- Decreased PT, muscle and MTU stiffness.    |
| Kubo et al., 2001 <sup>45</sup>                          | 7 male               | 10 min               | - Decreased tendon stiffness and hysteresis.   |
| Kubo, Kanehisa and Fukunaga, 2002a <sup>46</sup>         | 8 male               | 5 min                | - Decreased tendon stiffness and hysteresis.   |

d: day; s: seconds; min: minutes ROM: range of motion; PT: passive torque; MTU: muscle-tendon unit.

### Long-term Effects

Studies with chronic stretching protocols have increased ROM, but there are still few studies evaluating the effects on the tendon<sup>14,42</sup>.

Studies found in the literature (Table 2) do not present significant results regarding tendon stiffness. For example, Blazeovich et al.<sup>14</sup> and Konrad and Tilp (2014)<sup>41</sup> who applied four sets of 30 seconds, with three and six-week protocols, respectively, did not observe changes in the mechanical properties of the tendon nor did Kubo, Kanehisa and Fukunaga (2002b)<sup>48</sup>, when applying five sets of 45 seconds of stretching twice a day for approximately three weeks.

The fractionated protocols do not present an alteration in stiffness which may be due to the time of rest of the muscles between one and another stretching serie. These studies applied fractionated stretching protocols shorter than five minutes and found no change in tendon stiffness, nor did acute studies with these characteristics. Tendon stiffness decreased in acute studies with and continuously applied stretching protocols<sup>45,48</sup>, However, no chronic studies with this type of protocol were found to evaluate whether the results are similar.

Although chronic studies found no direct alteration in tendon stiffness, they present alteration in passive torque and MTJ displacement, outcomes that influence tendon stiffness.

Besides it not being clear in the literature whether change really occurs in tendon stiffness with stretching, it is also uncertain how the stretching protocol should be applied to change this variable. This gap in the literature thus justifies the need for controlled clinical studies with chronic stretching protocols that provide the scientific basis and information regarding the forms of conduct clearly for its application in clinical practice.

**Table 2** - Characterization of studies on the chronic effect of passive static stretching on the mechanical properties of the Achilles tendon.

| STUDY  | PARTICIPANTS        | PROTOCOL         | DURATION | RESULTS   |
|--|---------------------|------------------|----------|---|
| Blazevich et al., 2014 <sup>14</sup>             | 22 male             | 3 weeks, 2x/d    | 4 x 30 s | - Trend of the decreased MTJ displacement.<br>- No difference in tendon stiffness and PT. |
| Konrad and Tilp 2014 <sup>41</sup>               | 49, male and female | 6 weeks, 5d/week | 4 x 30 s | - Increased ROM.<br>- Without change in structural parameters of muscle and tendon.       |
| Kubo, Kanehisa and Fukunaga, 2002b <sup>48</sup> | 8 male              | 2.86 weeks, 2x/d | 5 x 45 s | - No difference in tendon stiffness.<br>- Decreased hysteresis.                           |
| Mahieu et al., 2007 <sup>42</sup>                | 96, male and female | 6 weeks, Dayli   | 5 x 20 s | - Decreased PT.<br>- No difference in tendon stiffness.                                   |

d: day; s: seconds; ROM: range of motion; PT: passive torque; MTJ: myotendinous junction.

## Conclusion

The literature presents several types of passive static stretching protocols with positive effect the increase of ROM, but with few identified changes in the mechanical muscle-tendon properties after the interventions.

The chronic response with fractional stretching for less than five minutes seems to be similar to the acute one and does not cause changes in tendon stiffness. Thus, there are two possible hypotheses: (1) longer stretching times may be necessary to generate changes in tendon stiffness, regardless of being fractional or continuous; or (2) the fact that the protocol is continuous, which influenced tendon stiffness, and shorter times of continuous application could produce the same effect.

## References

1. Garber CE, Blissmer B, Deschenes MR, Franklin BA, Lamonte MJ, Lee IM, et al. Quantity and quality of exercise for developing and maintaining cardiorespiratory, musculoskeletal, and neuromotor fitness in apparently healthy adults: guidance for prescribing exercise. *Med Sci in Spor.* 2011; 1334-1359.
2. Arampatzis A, Karamanidis K, Albracht K. Adaptational responses of the human Achilles tendon by modulation of the applied cyclic strain magnitude. *Journal of Experimental Biology.* 2007; 210:2743-2753.
3. Nordez A, Gross R, Andrade R, Le Sant G, Freitas S, Ellis R, et al. Non-Muscular Structures Can Limit the Maximal Joint Range of Motion during Stretching. *Sports Medicine.* 2017; 47(10):1925-1929.
4. Wepler CH, Magnusson SP. Increasing Muscle Extensibility: A matter of increasing length or modifying sensation? *Physical Therapy.* 2010; 90(3):438-449.
5. Kisner C, Colby LA. *Exercícios Terapêuticos Fundamentos e Técnicas.* Manole, São Paulo. 2005.
6. Herbert RD, Moseley AM, Butler JE, Gandevia SC. Change in length of relaxed muscle fascicles and tendons with knee and ankle movement in humans. *J Physiol.* 2002; 539.2:637–645.
7. Maffulli N, Almekinders LC. *The Achilles Tendon.* First Edition, Springer, 2007.
8. Nakamura M, Ikezoe T, Takeno Y, Ichihashi N. Acute and Prolonged Effect of Static Stretching on the Passive Stiffness of the Human Gastrocnemius Muscle Tendon Unit in Vivo. *J Orthop Res.* 2001; 29(11):1759-1763.
9. Kay AD, Blazeovich AJ. Moderate-duration static stretch reduces active and passive plantar flexor moment but not Achilles tendon stiffness or active muscle length. *J Appl Physiol.* 2009a; 106:1249–1256.
10. Kubo K, Kanehisa H, Fukunaga T. Effects of viscoelastic properties of tendon structures on stretch – shortening cycle exercise in vivo. *J Sports Sci.* 2005; 23(8):851- 860.
11. Witvrouw E, Mahieu N, Roosen P, McNair P. The role of stretching in tendon injuries. *Br J Sports Med.* 2007; 41:224-226.
12. Baranda OS, Ayala F. Chronic flexibility improvement after 12 week of stretching program utilizing the ACSM recommendations: hamstring flexibility. *Int J Sports Med.* 2010; 31: 389 – 396.

13. Arya, S, Kulig K. Tendinopathy alters mechanical and material properties of the Achilles tendon. *J Appl Physiol*. 2010; 108:670-675.
14. Blazeovich AJ, Cannavan D, Waugh CM, Miller SC, Thorlund JB, Aagaard P, et al. Range of motion, neuromechanical, and architectural adaptations to plantar flexor stretch training in humans. *J Appl Physiol*. 2014; 117:452–462.
15. Park DY, Rubenson J, Carr A, Mattson J, Besier T, Chou LB. Influence of Stretching and Warm-Up on Achilles Tendon Material Properties. *Foot Ankle Int*. 2011; 32(4):407-413.
16. Bayliss AJ, Weatherholt AM, Crandall TT, Farmer DL, McConnell JC, Crossley KM, et al. Achilles tendon material properties are greater in the jump leg of jumping athletes. *Musculoskelet Neuronal Interact*. 2016; 16(2):105-112.
17. Gajdosik RL, Vander LDW, Williams AK. Influence of age on length and passive elastic stiffness characteristics of the calf muscle-tendon unit of women. *Phys Ther*. 1999; 79(9):827-38.
18. Radford JA, Burns J, Buchbinder R, Landorf KB, Cook C. Does stretching increase ankle dorsiflexion range of motion? A systematic review. *Br J Sports Med*. 2006; 40:870–875.
19. Muramatsu T, Muraoka T, Takeshita D, Kawakami Y, Hirano Y, Fukunaga T. Mechanical properties of tendon and aponeurosis of human gastrocnemius muscle in vivo. *J Appl Physiol*. 2001; 90:1671–1678.
20. Cretnik A. Achilles tendon. First published, InTech, Croácia. 2012
21. Buchanan CI, Marshb RL. Effects of exercise on the biomechanical, biochemical and structural properties of tendons. *Comp Biochem Phys*. 2002; A Part A(133):1101–1107.
22. Tardioli A, Malliaras P, Maffulli N. Immediate and short-term effects of exercise on tendon structure: biochemical, biomechanical and imaging responses. *Br Med Bull*. 2012; 103:169–202.
23. Magnusson SP, Aagard P, Simonsen E, Bojsen-Moller F. A biomechanical evaluation of cyclic and static stretch in human skeletal muscle. *Int J Sports Med*. 1998; 19(5):310–316.
24. Aslan H, Kimelman-Bleich N, Pelled G, Gazit D. Molecular targets for tendon neoformation. *J Clin Invest*. 2008; 118(2):439-444.
25. Doral MN, Alam M, Bozkurt M, Turhan E, Atay AO, Donmez G, et al. Functional anatomy of the Achilles tendon. *Knee Surg Sports Traumatol Arthrosc*. 2010; 18(5):638-643.
26. Maganaris CN, Narici MV, Maffulli N. Biomechanics of the Achilles tendon. *Disabil Rehabil*. 2008; 30(20–22):1542–1547.
27. Butler DL, Grood ES, Noyes FK, Zernicke RF. Biomechanics of ligaments and tendons. *Exerc Sport Sci Rev*. 1978; 6:125– 181.
28. Thacker SB, Gilchrist J, Stroup DF, Kimsey D Jr. The Impact of Stretching on Sports Injury Risk: A Systematic Review of the Literature. *Med Sci Sports Exerc*. 2004; 36(3): 371–378.
29. Small K, Naughton LMC, Matthews M. A Systematic Review into the Efficacy of Static Stretching as Part of a Warm-Up for the Prevention of Exercise-Related Injury. *Res Sports Med*. 2008; 16(3):213-231.
30. Smith CA. The warm-up procedure: to stretch or not to stretch. A brief review. *J Orthop Sports Phys Ther*. 1994; 19(1):12-17.
31. Bandy WD, Irion JM. The Effect of Time on Static Stretch on the Flexibility of the Hamstring Muscles. *Phys Ther*. 1994; 74(S):54–59.
32. Davis DS, Ashby PE, McCaule KL, McQuain JA, Wine JM. The effectiveness of 3 stretching techniques on hamstring flexibility using consistent stretching parameters. *J Strength Cond Res*. 2005; 19(1):27-32.

33. Chan SP, Hong Y, Robinson PD. Flexibility and passive resistance of the hamstrings of young adults using two different static stretching protocols. *Scand J Med Sci Sport*. 2001; 11:81-86.
34. Covert CA, Alexander MP, Petronis JJ, Davis DS. Comparison of ballistic and static stretching on hamstring muscle length using an equal stretching dose. *J Strength Cond Res*. 2010; 24(11):3008–3014, 2010.
35. Gajdosik RL. Passive extensibility of skeletal muscle: review of the literature with clinical implications. *Clin Biomech*. 2001; 16:87-101.
36. Magnusson SP, Simonsen EB, Aagaard P, Kjaer M. A mechanism for altered flexibility in human skeletal muscle. *J Physiol*. 1996; 497(2):291-298.
37. Morse CI, Degens H, Seynnes OR, Maganaris CN, Jones DA. The acute effect of stretching on the passive stiffness of the human gastrocnemius muscle tendon unit. *J Physiol*. 2008; 586.1: 97–106.
38. Ryan ED, Beck TW, Herda TJ, Hull HR, Hartman MJ, Costa PB, et al. The Time Course of Musculotendinous Stiffness Responses Following Different Durations of Passive Stretching. *J Orthop Sports Phys Ther*. 2008; 38(10):632-639.
39. Konrad A, Stafilidis S, Tilp M. Effects of acute static, ballistic, and PNF stretching exercise on the muscle and tendon tissue properties. *Scand J Med Sci Sports*. 2017; 27(10):1070-1080.
40. Nakamura M, Ikezoe T, Takeno Y, Ichihashi, N. Time course of changes in passive properties of the gastrocnemius muscle-tendon unit during 5 min of static stretching. *Man Ther*. 2013; 18(3):211-215.
41. Konrad A, Tilp M. Increased range of motion after static stretching is not due to changes in muscle and tendon structures. *Clin Biomech*. 2014; 29:636–642.
42. Mahieu NN, McNair P, Muynck M, Stevens V, Blanckaert I, Smits N, et al. Effect of Static and Ballistic Stretching on the Muscle-Tendon Tissue Properties. *Med Sci Sports Exerc*. 2007; 39(3):494–501.
43. McNair PJ, Dombroski EW, Hewson DJ, Stanley SN. Stretching at the ankle joint: viscoelastic responses to holds and continuous passive motion. *Med Sci Sports Exerc*. 2001; 33:354-358.
44. Fowles JR, Sale DG, MacDougall JD. Reduced strength after passive stretch of the human plantarflexors. *J Appl Physiol*. 2000; 89:1179- 1188.
45. Kubo K, Kanehisa H, Fukunaga T. Is passive stiffness in human muscles related to the elasticity of tendon structures? *Eur J Appl Physiol*. 2001; 85:226-232.
46. Kubo K, Kanehisa H, Fukunaga T. Effects of transient muscle contractions and stretching on the tendon structures in vivo. *Acta Physiol Scand*. 2002a; 175(2):157-164.
47. Kay AD, Beasley JH, Blazeovich AJ. Effects of Contract–Relax, Static Stretching, and Isometric Contractions on Muscle–Tendon Mechanics. *Med Sci Sports Exerc*. 2015; 47(10):2181–2190.
48. Kubo K, Kanehisa H, Fukunaga T. Effect of stretching training on the viscoelastic properties of human tendon structures in vivo. *J Appl Physiol*. 2002b; 92:595-601.